

# HUMAN POSTURE AND MOVEMENT PREDICTION BASED ON MUSCULOSKELETAL MODELING

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## **Introduction**

- Motivation
- Human models
- Simulation models
- State-of-the-art

## **Posture and movement Prediction using inverse-inverse dynamics**

- Parameterization
- Objective function
- Optimization
- Validation

## **Results**

- Example I
- Example II
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## **Concluding remarks**

## **Future works**

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## Digital manikins applications:

- ✓ Orthopedic
  - ✓ Rehabilitation
  - ✓ Clinical bi
  - ✓ Ergonomics
  - ✓ Occupational
  - ✓ Industrial
  - ✓ Sports equipment
- The digital manikin must be driven by experimental kinematic and kinetic data!
- Performance optimization

## Experiment limitations:

- Time-consuming
- Technically difficult
- Potentially unsafe
- Expensive

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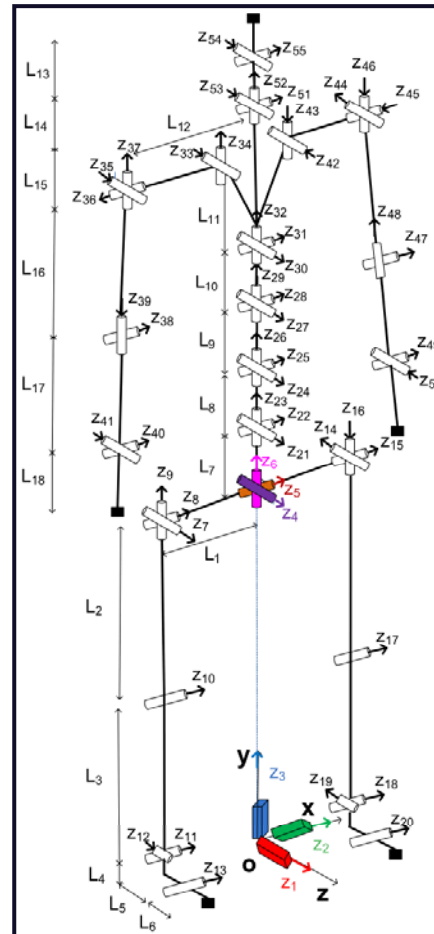
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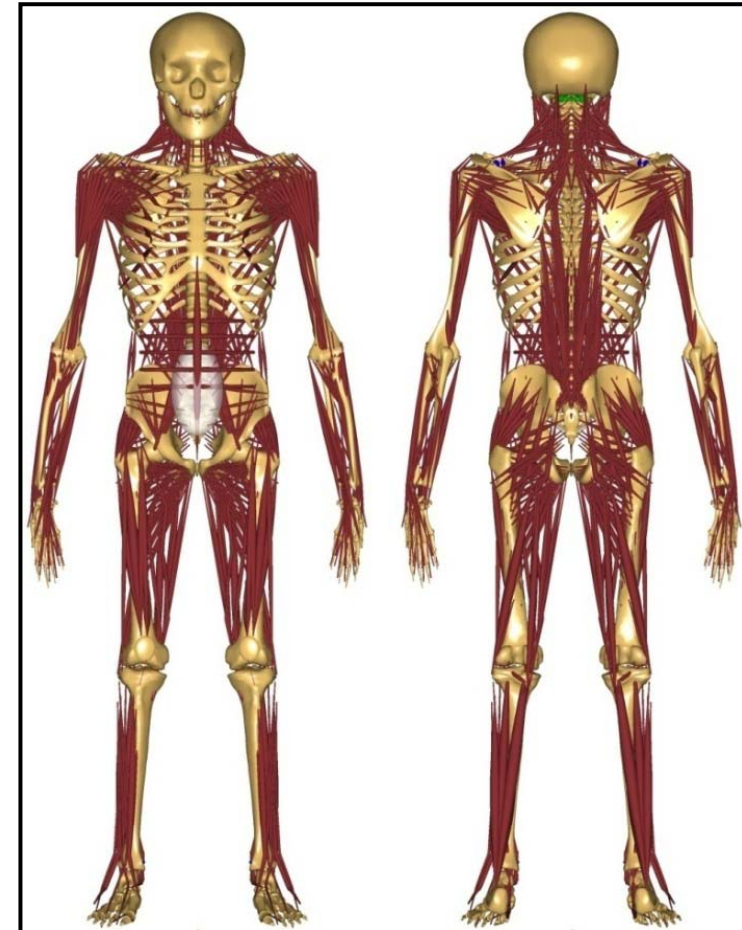
### Joint torque model



Digital human skeletal model (Xiang et al., 2010)

Series of rigid segments connected by one or more revolute joints.

### AnyBody Musculoskeletal Model



Written in a general scripting language

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## Why do we need simulation models?

Direct measurement of muscle force as a fundamental requirement for movement study is restricted to invasive measurement!

## Types of simulation model:

- Forward dynamics
- Inverse dynamics

### Redundancy problem

There are more muscles than necessary to generate the motions.



### Optimization

Minimization of an appropriate cost function is necessary to cope with the redundancy of muscular load-sharing.

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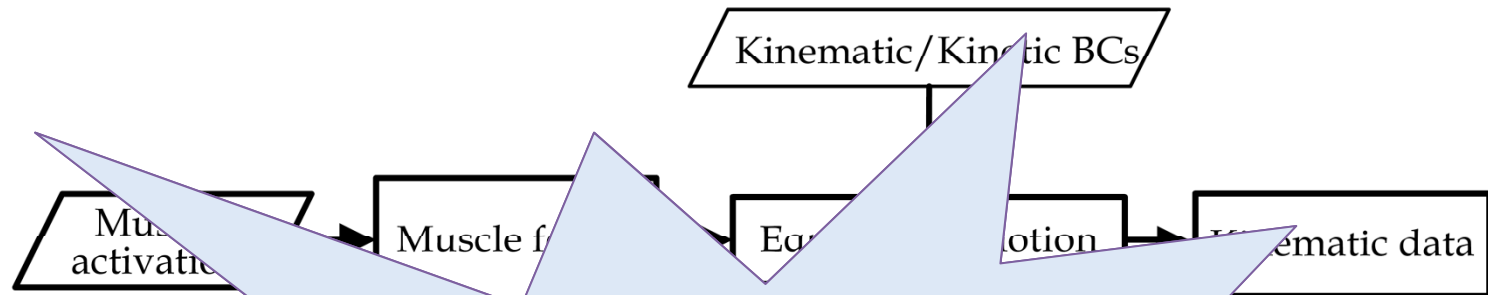
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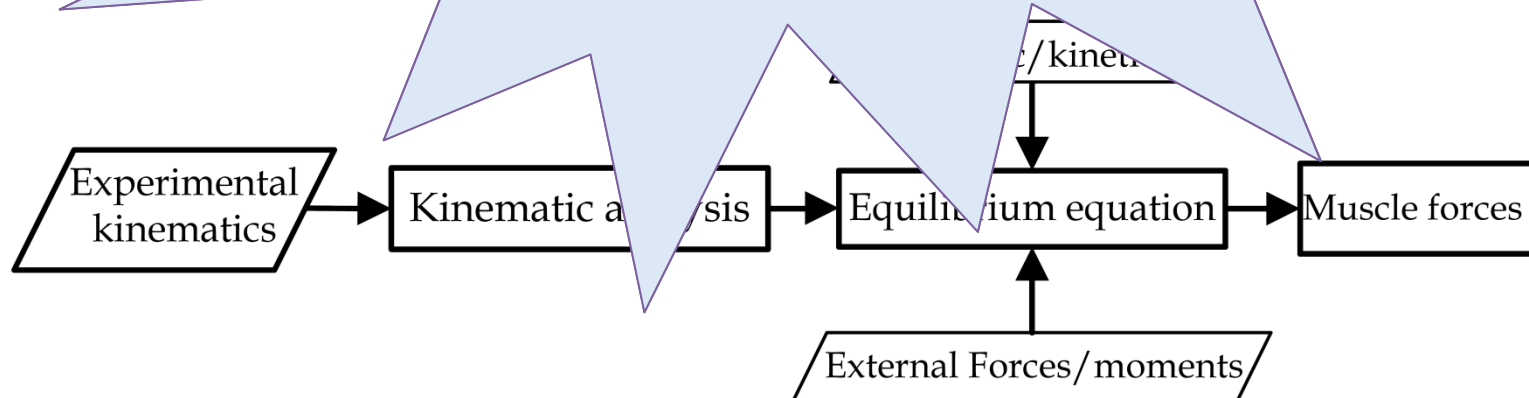
## Future works

### ○ Forward dynamics



**In many practical simulation cases, neither the muscle forces nor the motion is known a-priori!**

### ○ Inverse



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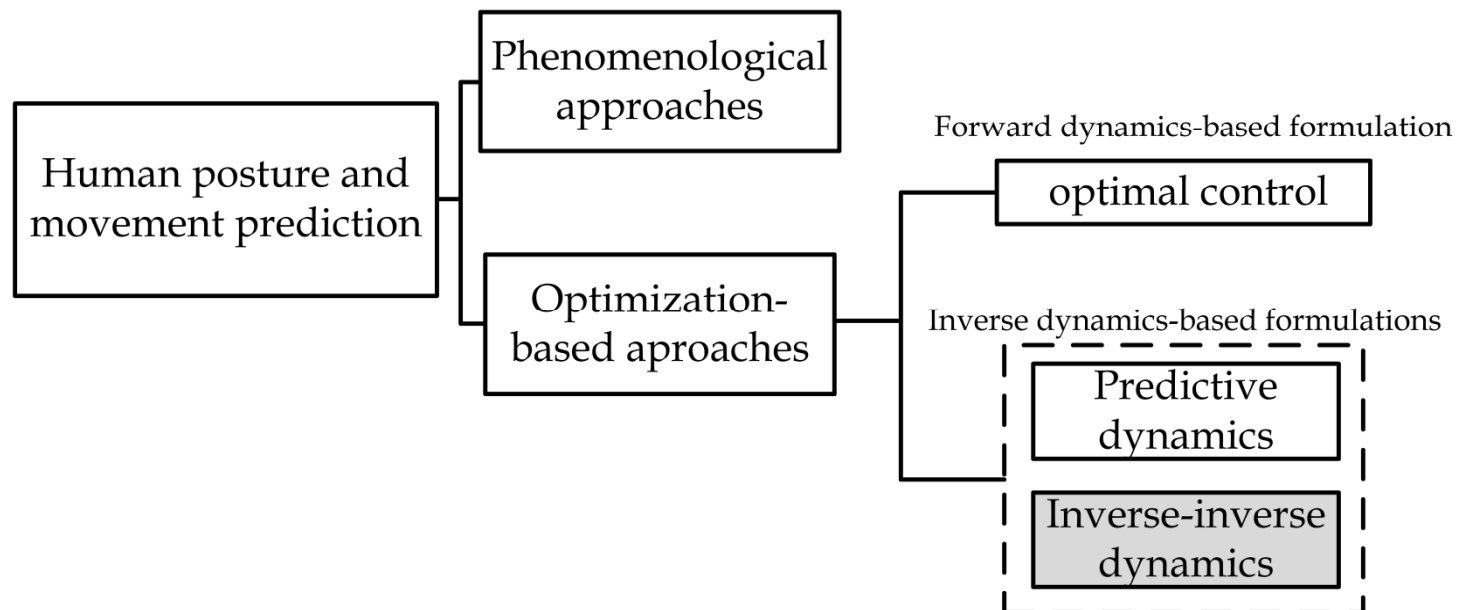
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## Research questions

- I. Can we resolve the indeterminacy by formulating the human movement as an optimization problem?
- II. What is the objective function?
- III. Does any single formulation predict a wide range of human posture/movements?



The novelty of inverse-inverse dynamics is to generalize the idea of using an inverse dynamics-based formulation for human posture and movement prediction by using a detailed musculoskeletal model.

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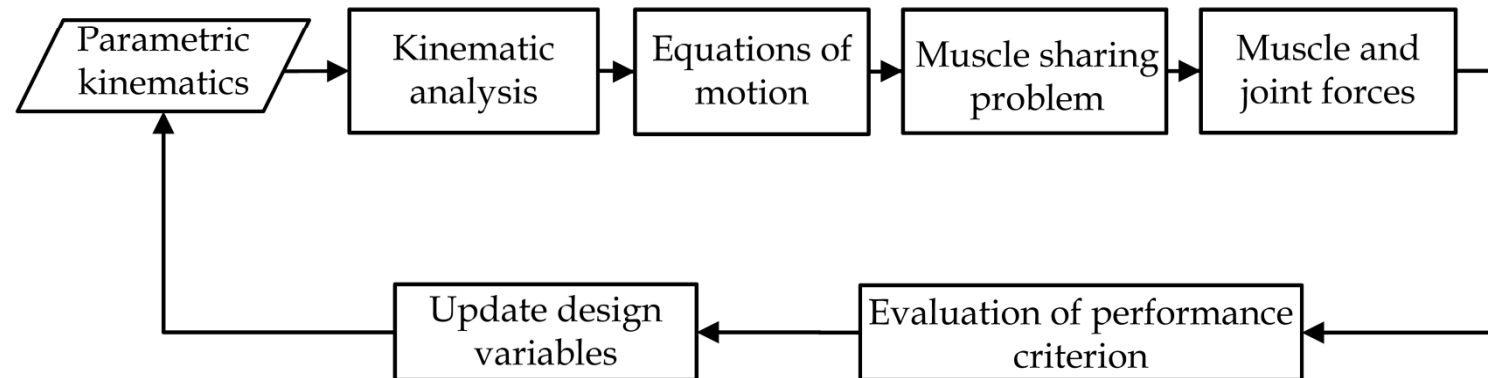
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## Inverse-inverse dynamics



**Find:**  $q_i, \quad i \in \{1, \dots, n^{(C)}\}$

**To:** **minimize** performance criterion

**S.t:**  $\left\{ \begin{array}{l} \text{Anatomical joint angle limits:} \quad \theta_i^L \leq \theta_i \leq \theta_i^U, \quad i \in \{1, \dots, n^{(D)}\} \\ \text{Muscle strength:} \quad 0 \leq f_i^{(M)} \leq N_i, \quad i \in \{1, \dots, n^{(M)}\} \\ \text{Dynamic Stability} \\ \text{Obstacle and Self avoidance} \\ \text{Environmental Constraints} \end{array} \right\}$



# Movement parameterization

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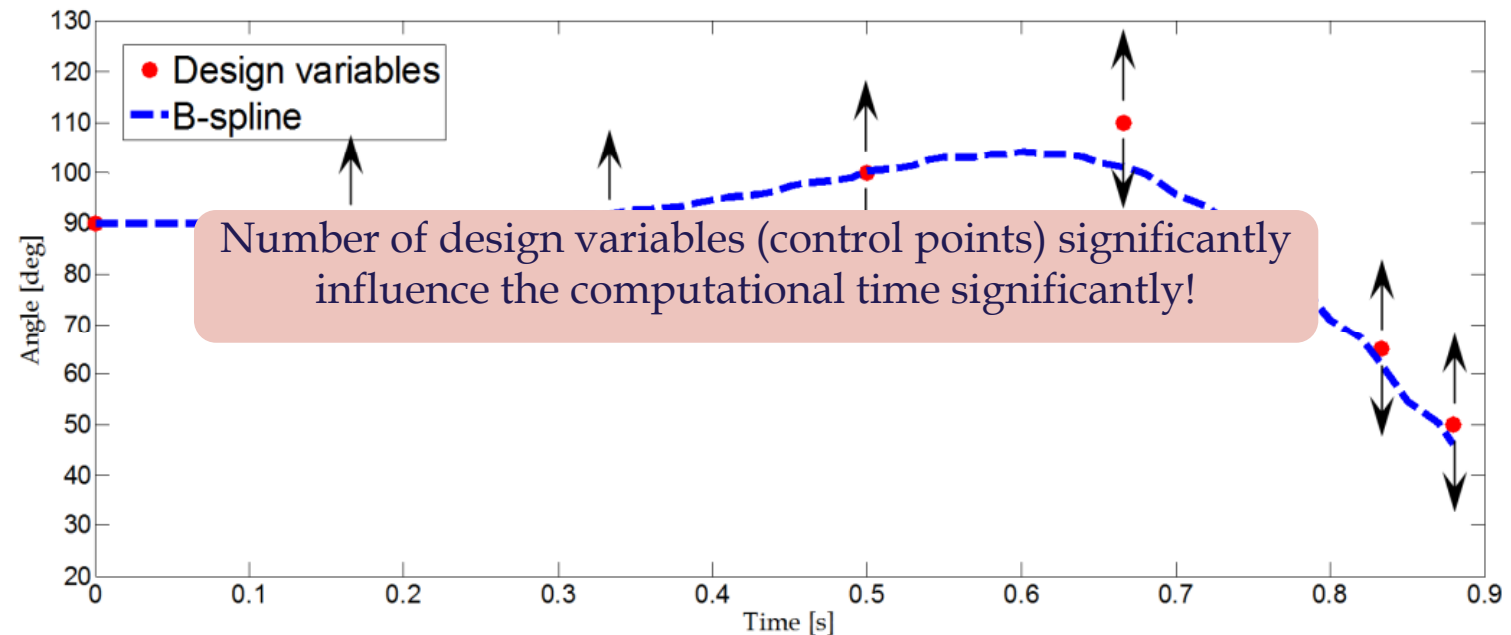
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The joint angles are parameterized by means of time functions controlling the motion. Time function could be B-spline, Polynomial, Fourier series and etc.



- ❑ Identification of the level of parameterization complexity remains a challenging task.
- ❑ The machine parameters can be considered as design variables.

# Objective function definition

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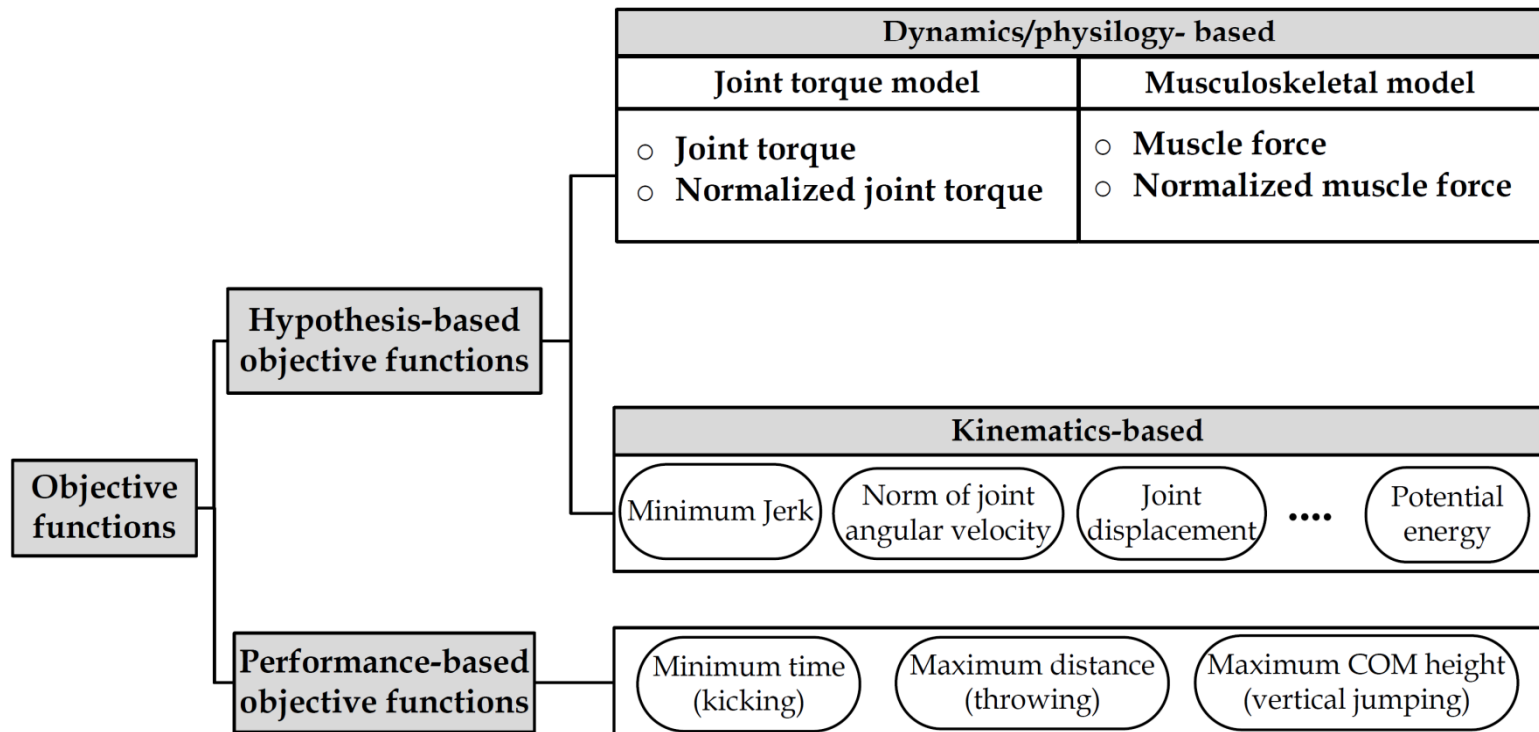
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The optimality hypothesis in human movement prediction is that movements are planned to optimize a performance criterion.



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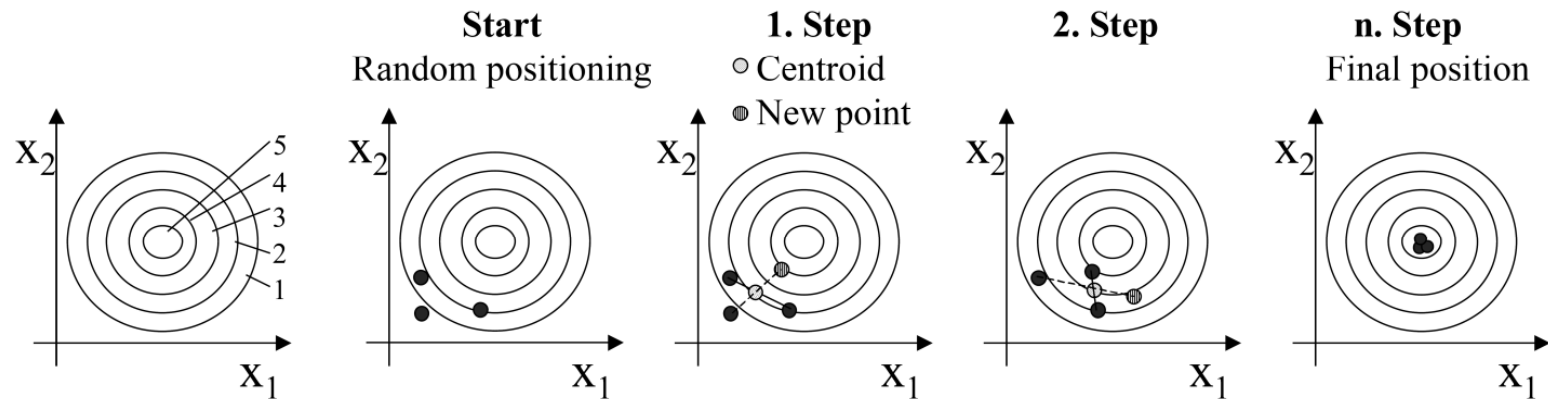
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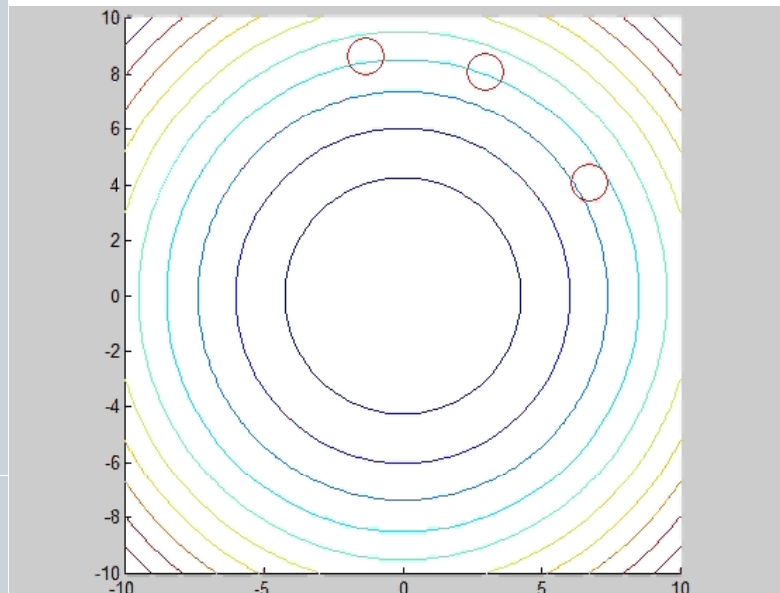
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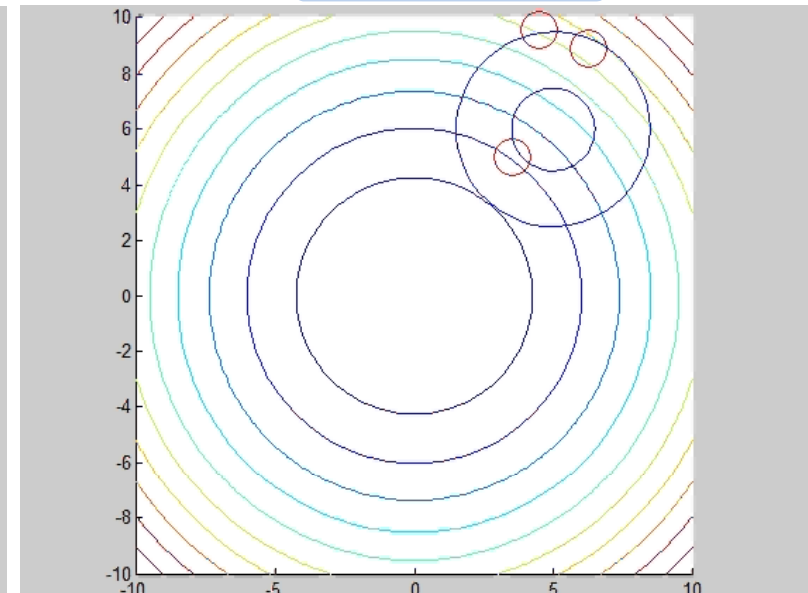
Complex method: a non-gradient optimization technique!



Unconstrained



Constrained



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## Error quantification

A quantitative validation metric originally proposed by Geers (1984) was used to quantify the differences between the predicted and measured results.

$$M = \sqrt{\frac{v_{cc}}{v_{mm}} - 1}$$

$$P = \frac{1}{\pi} \arccos\left(\frac{v_{mc}}{\sqrt{v_{mm}v_{cc}}}\right)$$

$$C = \sqrt{M^2 + P^2}$$

$$v_{mm} = \frac{1}{t_2 - t_1} \int_{t_1}^{t_2} m(t)^2 dt$$

$$v_{cc} = \frac{1}{t_2 - t_1} \int_{t_1}^{t_2} c(t)^2 dt$$

$$v_{mc} = \frac{1}{t_2 - t_1} \int_{t_1}^{t_2} m(t)c(t) dt$$

If the experimental data and computational results are identical,  $M$ ,  $P$  and  $C$  will be zero!

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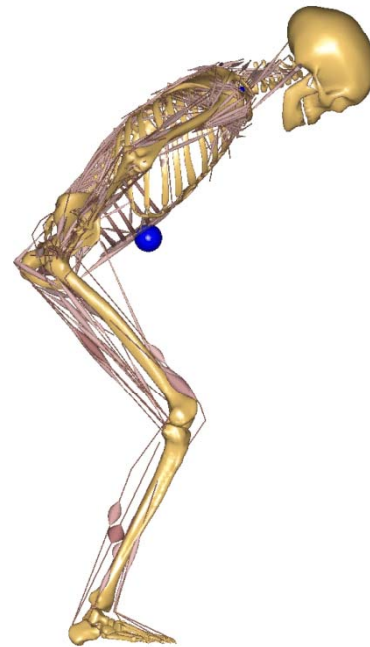
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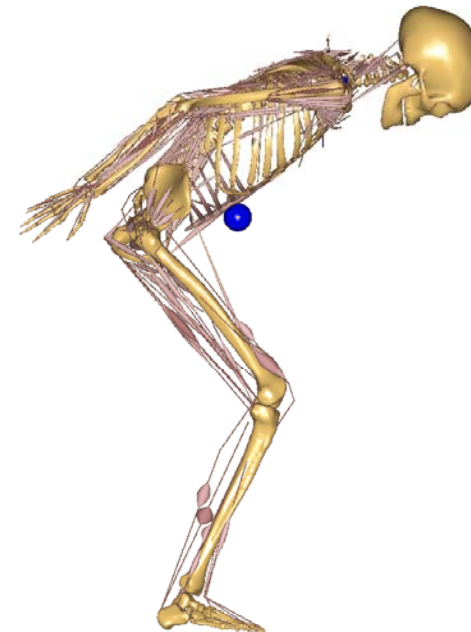
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Can we formulate the human movement prediction as an optimization problem?



SVJ



SVJA

# Human modeling and parameterization

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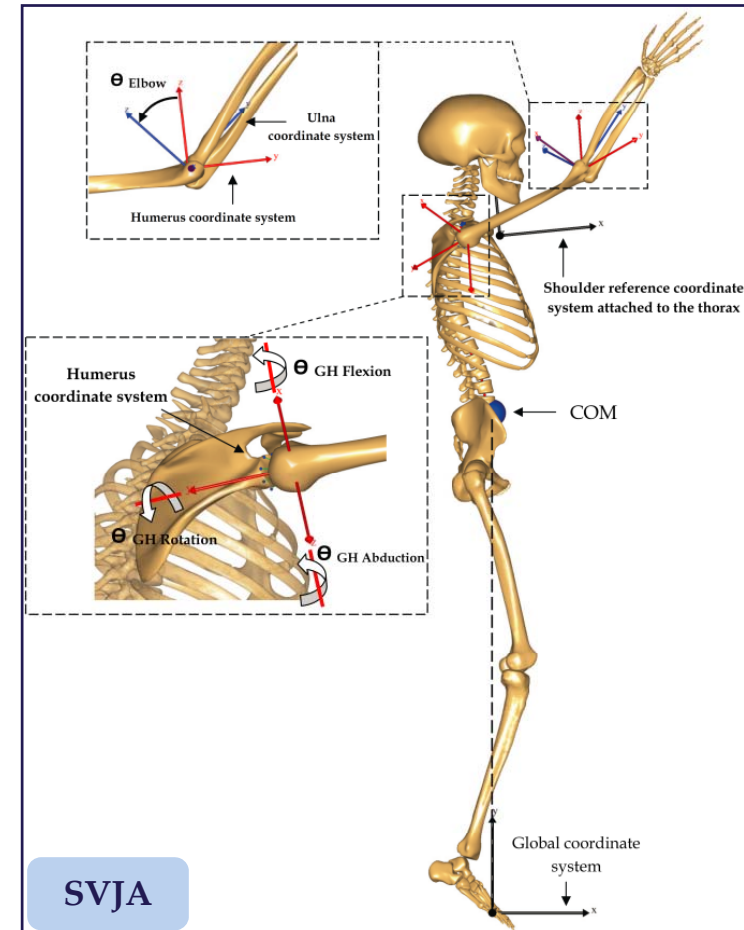
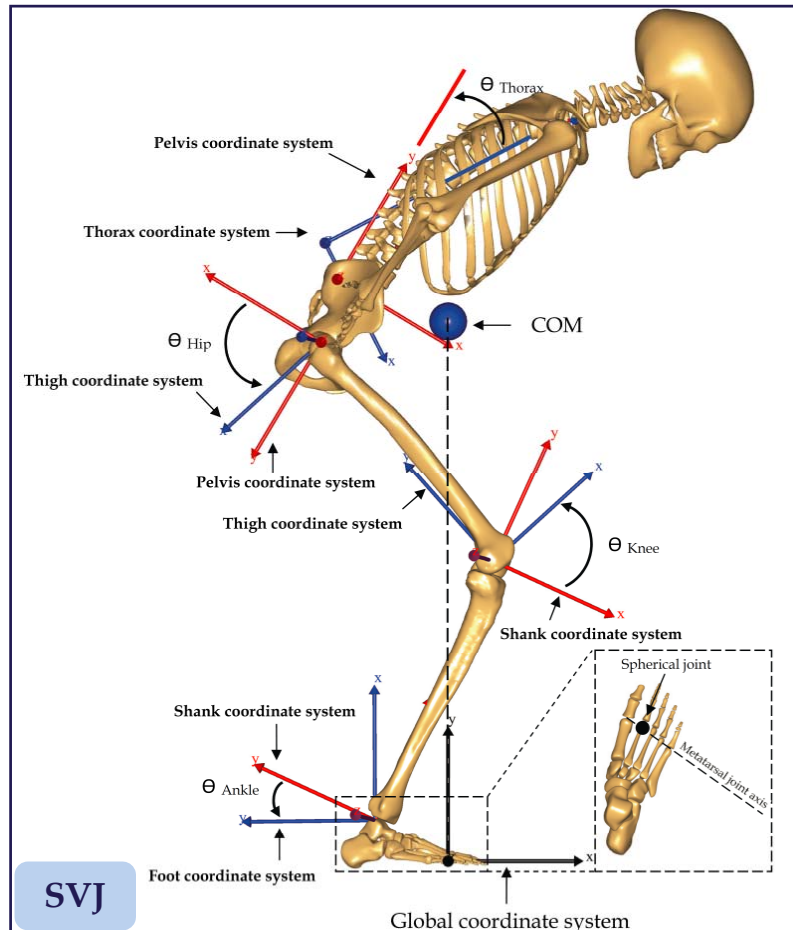
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We used **12** control points for each joint angle to discretize the motion over the entire jumping time by means of a fourth order **B-spline** curve.

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- Objective function for the movement prediction:

$$F = Y_{\text{COM@take-off}} + (V_{\text{COM@take-off}})^2 / 2g$$

- Optimization:

Find:  $q_i, \quad i \in \{1, \dots, n^{(C)}\}$

To: minimize  $-(Y_{\text{COM@take-off}} + (V_{\text{COM@take-off}})^2 / 2g)$

$$\theta_i^L \leq \theta_i \leq \theta_i^U, \quad i \in \{1, \dots, n^{(D)}\}$$

S.t:  $0 \leq f_i^{(M)} \leq N_i, \quad i \in \{1, \dots, n^{(M)}\}$



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## Experimental study

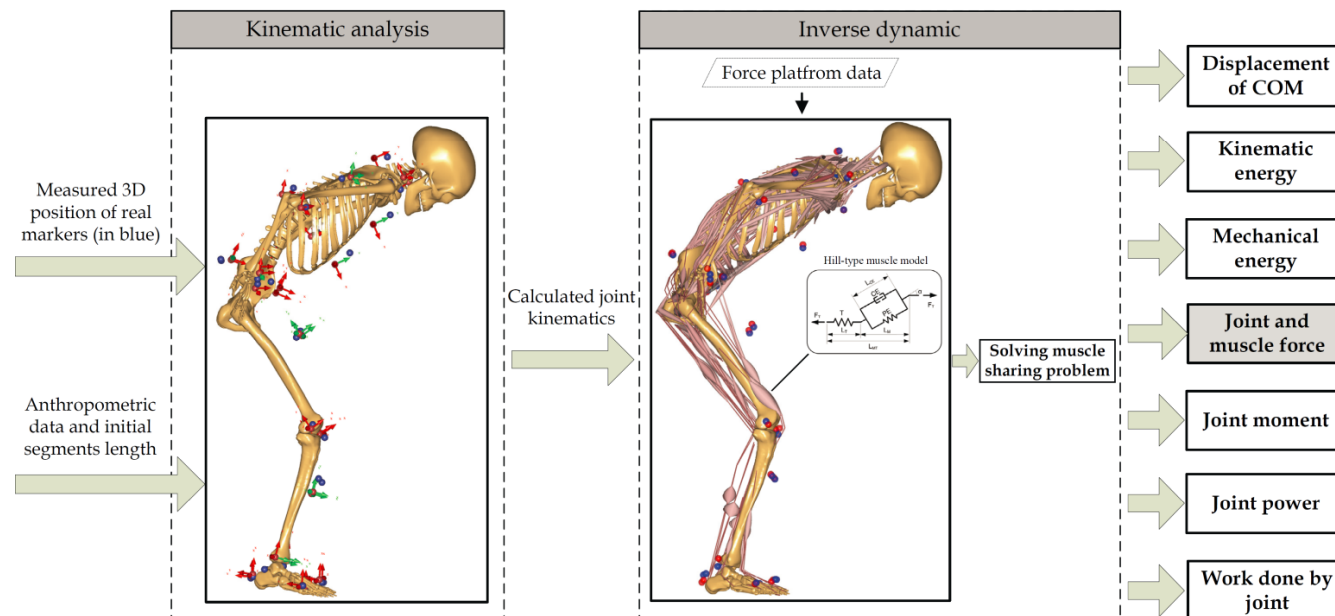
Subjects: A group of six healthy males volunteered for the test.

### Instrumentation:

- **39** reflective skin markers
- Two adjacent force platforms (sampling at 1000 Hz).
- Eight infrared cameras (sampling at 250 Hz)

### Test protocol:

- Squat vertical jumping (6 trials)
- Squat vertical jumping with arm swing (6 trials)
- The data set comprised 6 (subjects) × 5 (trials) × 2 (test conditions)





# Results ...

The predicted jumping time in SVJ and SVJA is **0.570 (s)** and **0.573 (s)** respectively

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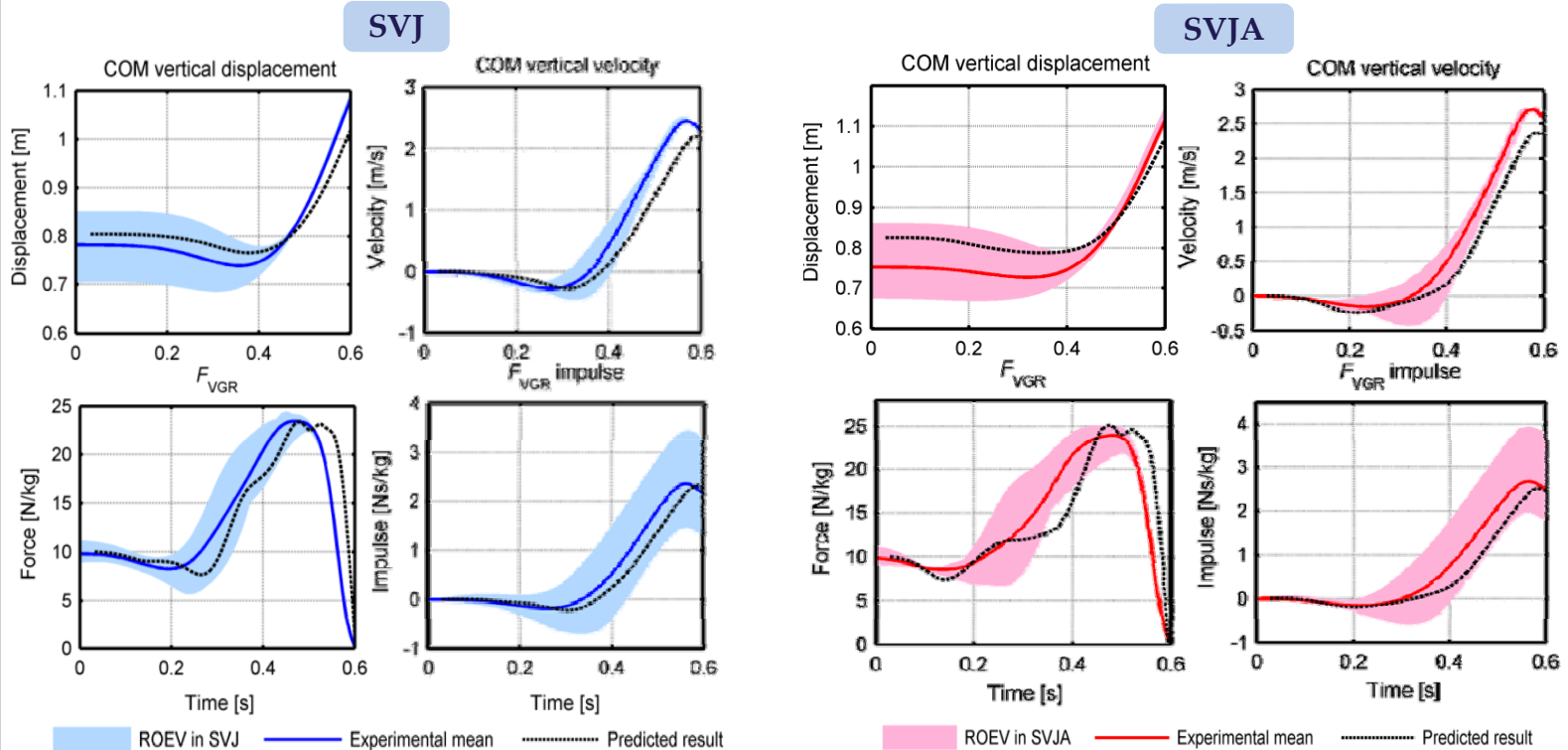
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		NRMSE	$r^2$	$M$	$P$	$C$
SVJ	COM vertical displacement (m)	0.082	0.985	0.011	0.011	0.015
	COM vertical velocity ( $\text{ms}^{-1}$ )	0.096	0.976	-0.206	0.047	0.211
	$F_{VGR}$ ( $\text{Nkg}^{-1}$ )	0.122	0.791	0.004	0.061	0.061
	$F_{VGR}$ impulse ( $\text{Nskg}^{-1}$ )	0.079	0.973	-0.125	0.048	0.134
SVJA	COM vertical displacement (m)	0.150	0.952	0.049	0.017	0.052
	COM vertical velocity ( $\text{ms}^{-1}$ )	0.099	0.982	-0.208	0.048	0.214
	$F_{VGR}$ ( $\text{Nkg}^{-1}$ )	0.155	0.701	-0.006	0.078	0.078
	$F_{VGR}$ impulse ( $\text{Nskg}^{-1}$ )	0.118	0.955	-0.201	0.065	0.211

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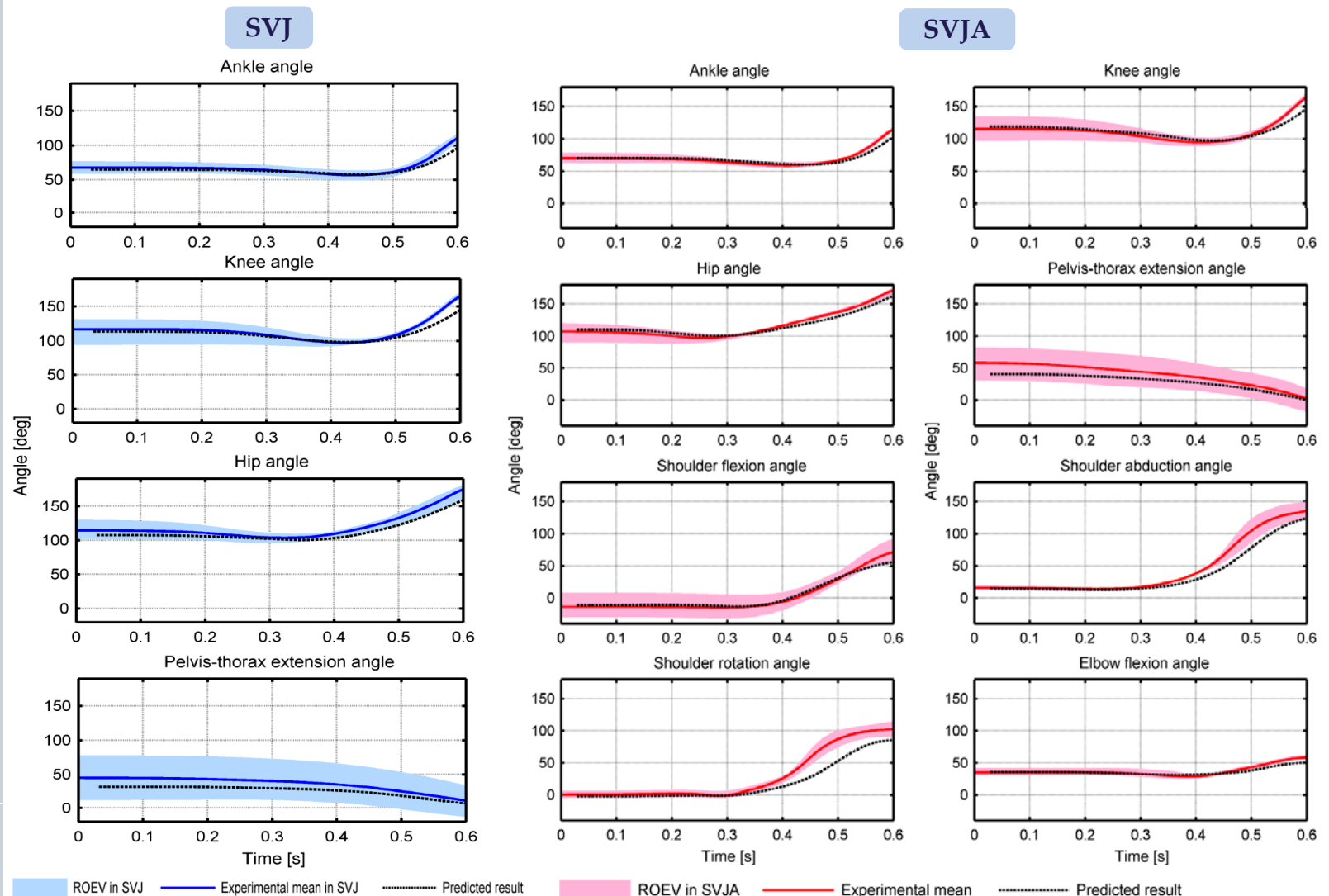
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Predicted and experimental values of the joint angles in SVJA and SVJA.



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		NRMSE	$r^2$	$M$	$P$	$C$
SVJ	Ankle angle (deg)	0.067	0.997	-0.038	0.012	0.040
	Knee angle (deg)	0.080	0.990	-0.033	0.011	0.035
	Hip angle (deg)	0.102	0.995	-0.058	0.006	0.058
						0.273
SVJA						0.025
	Pelvis-thorax angle (deg)	0.200	0.991	-0.263	0.011	0.263
	Shoulder flexion angle (deg)	0.053	0.991	-0.150	0.031	0.153
	Shoulder abduction angle (deg)	0.107	0.980	-0.190	0.031	0.192
	Shoulder rotation angle (deg)	0.162	0.956	-0.306	0.064	0.312
	Elbow flexion angle (deg)	0.112	0.965	-0.040	0.025	0.047

Inverse-inverse dynamics can reproduce the coordinated motion .

Predicted and experimental mean of the  $Y_{COM@take-off}$ ,  $V_{COM@take-off}$  and jump height in SVJA and SVJ.

	Averaged experimental results			Predicted results		
	SVJ	SVJA	Enhancement (%)	SVJ	SVJA	Enhancement (%)
$Y_{COM@take-off}$						8
$V_{COM@take-off}$						
jump height						6

This approach is also capable of predicting the jump height enhancement in squat vertical jumping with arm swing.

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What is the optimization criterion for a movement under investigation?



Musculoskeletal model of a bicycle rider with 176.6 cm height and 69.8 kg weight

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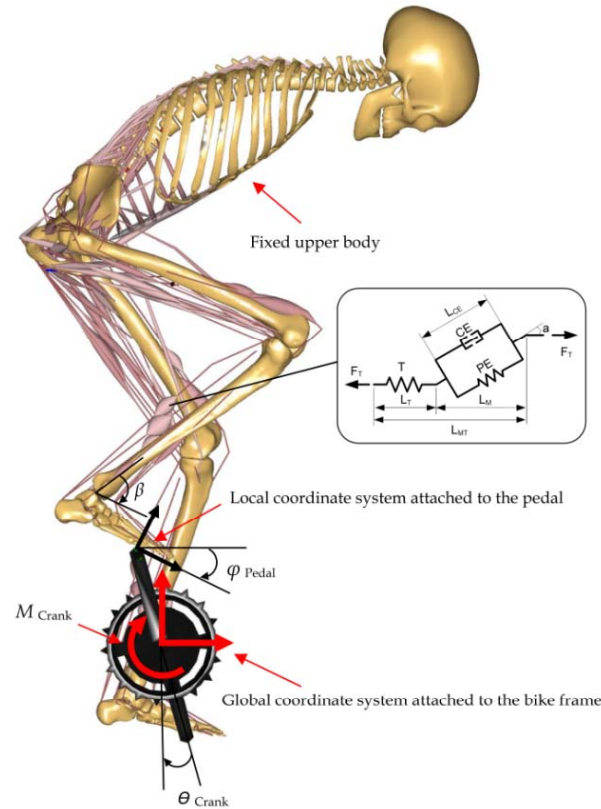
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□ Objective function:

$$F = \frac{1}{T} \int_0^T \left[ p \sqrt{\sum_{i=1}^n \left( \frac{f_i^{(M)}}{N_i} \right)^p} \right]^q dt$$

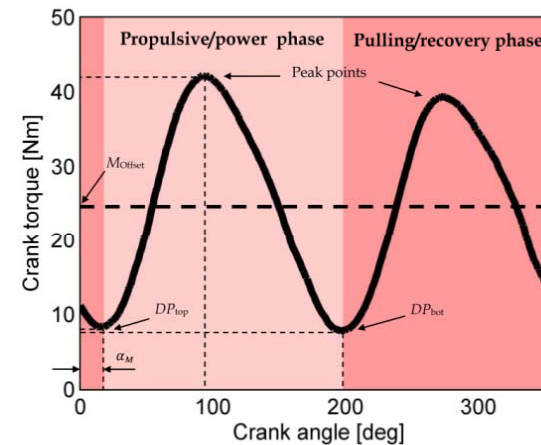
$$p, q \in \{1, 2, 3, 4, 5\}$$

$$F = \max_t \max_i \left( \frac{f_i^{(M)}}{N_i} \right)$$

$$\varphi_{\text{Pedal}} = \sum_{i=1}^3 [A_i \cos(\omega_i t) + B_i \sin(\omega_i t)]$$

$$\omega_i = (i - 1)2\pi f$$

$$\mathbf{A} = [A_1, A_2, A_3]; \quad \mathbf{B} = [B_1, B_2, B_3]$$



$$M_{\text{Crank}} = M_{\text{Offset}} + (M_{\text{Offset}} - M_{\text{DP}_{\text{top}}}) \sin(4\pi f t + \alpha_M)$$

□ Optimization:

Find:  $\{A_1, A_2, A_3, B_1, B_2, B_3, M_{\text{DP}_{\text{top}}}, \alpha_M\}$

To: minimize  $F$

S.t:  $\beta_{\text{lower}} \leq \beta \leq \beta_{\text{upper}}$   
 $0 \leq f_i^{(M)} \leq N_i, \quad i \in \{1, \dots, n^{(M)}\}$



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## Experimental study

Subjects: A group of nine male cyclists volunteered for the test (with their own bike)

Instrumentation:

The output power and pedaling cadence were sampled at 10 Hz using SRM.

Test protocol:

- Three tests on level terrain and three tests on uphill terrain (4.8% grade).
- One test with preferred gear ratio, the two other tests with one gear ratio above and one gear ratio below the preferred gear ratio.
- All test were performed during **1 min** at a power output representing 90% peak power output.

Mean pedaling cadence and power output of the cyclists during experimental conditions

Cycling condition	Pedaling cadence $\pm$ SD (rpm)	Power output $\pm$ SD (W)
level terrain at low cadence (LL)	87.8 $\pm$ 8.8	240 $\pm$ 16.8
level terrain at preferred cadence (LP)	94.7 $\pm$ 8.2	239.5 $\pm$ 18.8
level terrain at high cadence (LH)	101.9 $\pm$ 8.3	238.9 $\pm$ 17.9
Uphill terrain at low cadence (UL)	74.9 $\pm$ 9.5	245.2 $\pm$ 12.2
Uphill terrain at preferred cadence (UP)	82.2 $\pm$ 12.0	246.5 $\pm$ 14.7
Uphill terrain at high cadence (UH)	87.7 $\pm$ 13.0	242.8 $\pm$ 14.6

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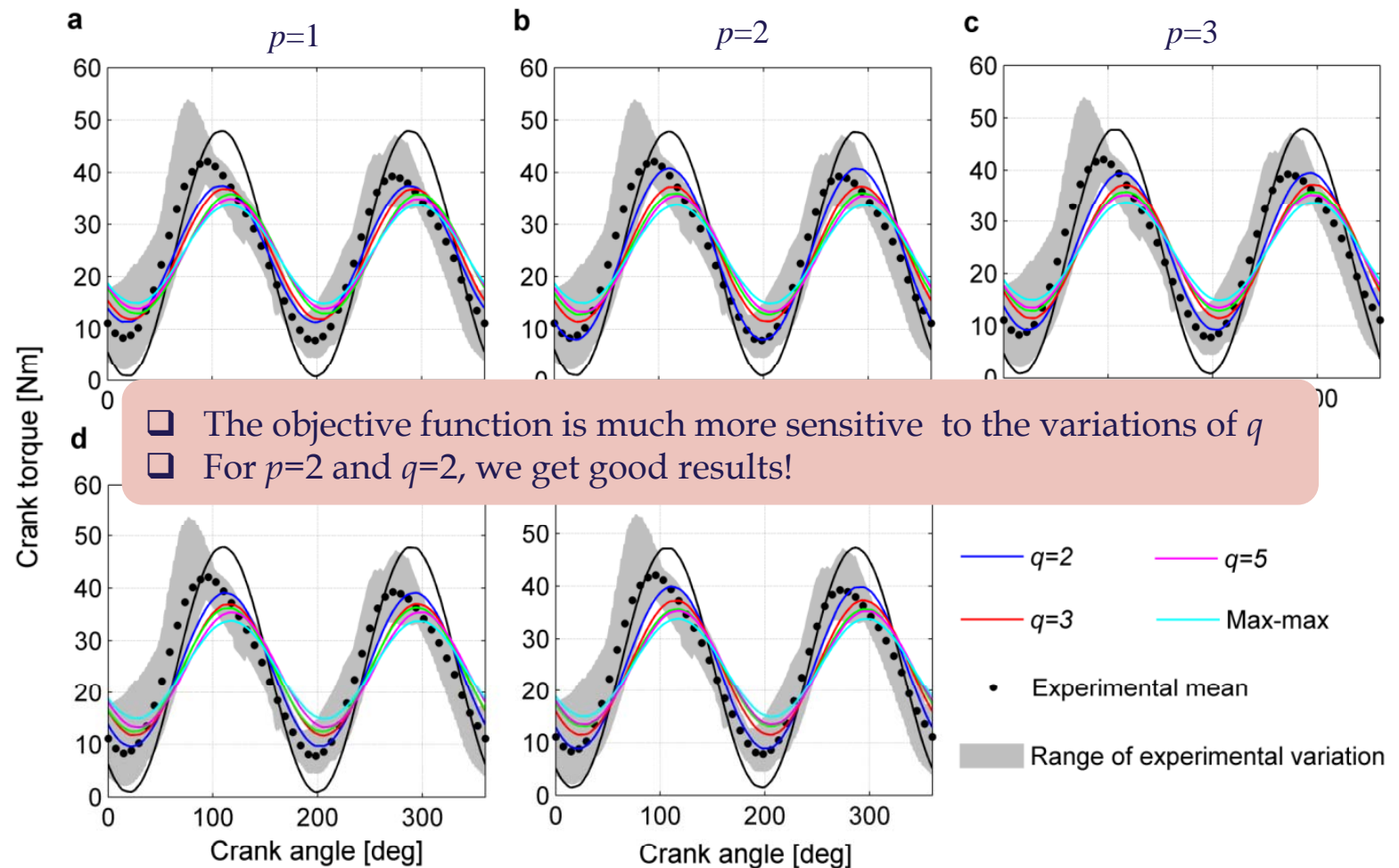
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Predicted and experimental data for pedaling on level terrain at preferred cadence



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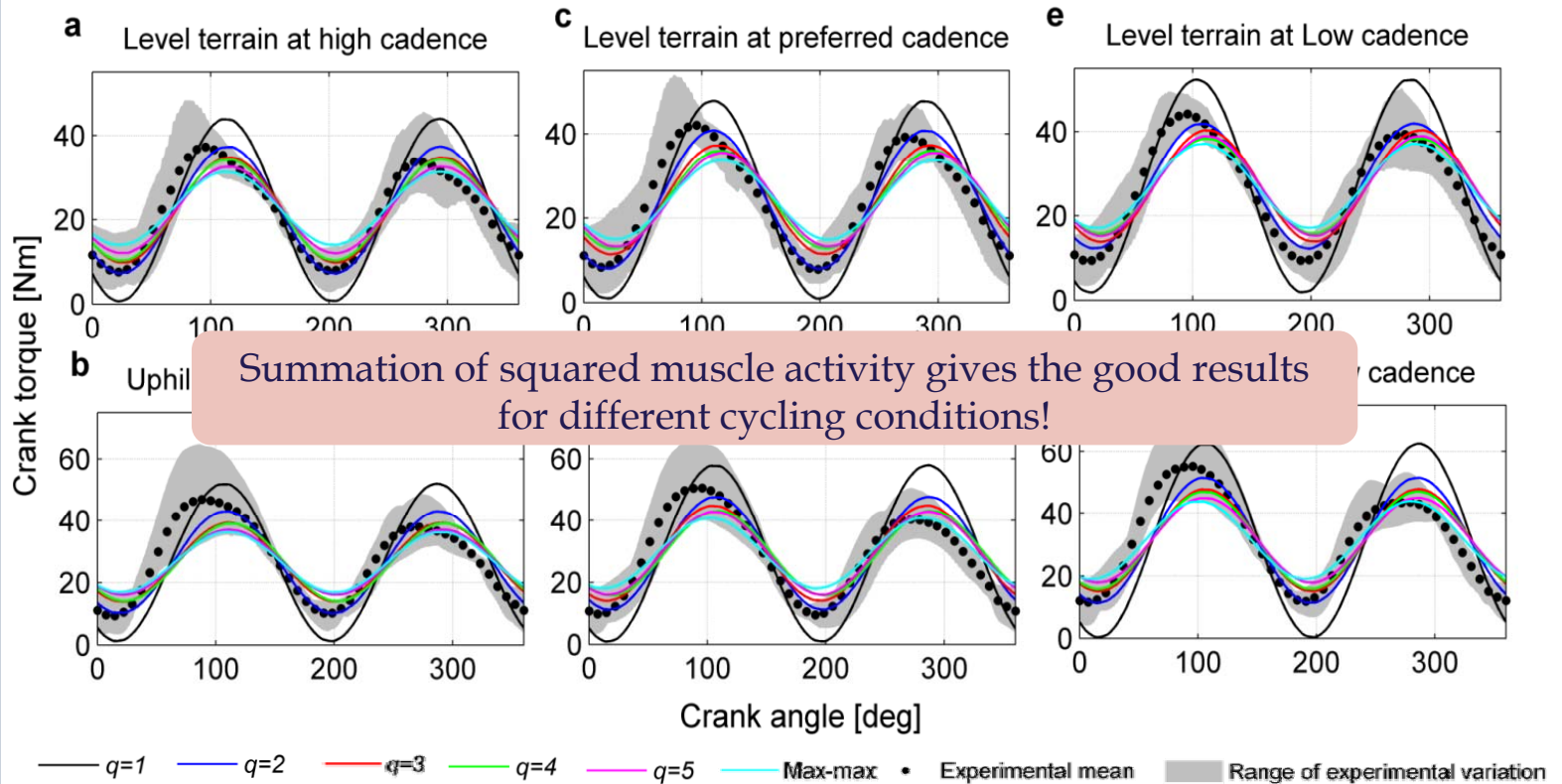
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Averaged errors for all cycling conditions ( $p=2$ )

	$q=1$	$q=2$	$q=3$	$q=4$	$q=5$	Max-max
Mean NRMSE $\pm$ SD	0.222	0.125	0.146	0.158	0.162	0.167
Mean $r^2 \pm$ SD	0.849	0.878	0.810	0.787	0.788	0.843
Mean $M \pm$ SD	0.098	0.018	0.034	0.042	0.049	0.057
Mean $P \pm$ SD	0.079	0.050	0.058	0.063	0.065	0.066
Mean $C \pm$ SD	0.127	0.052	0.069	0.077	0.083	0.088



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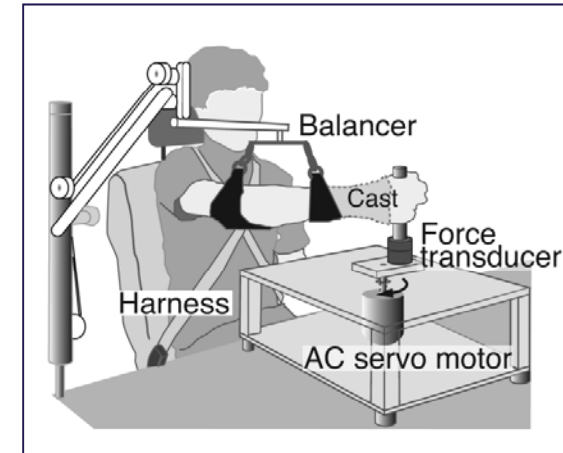
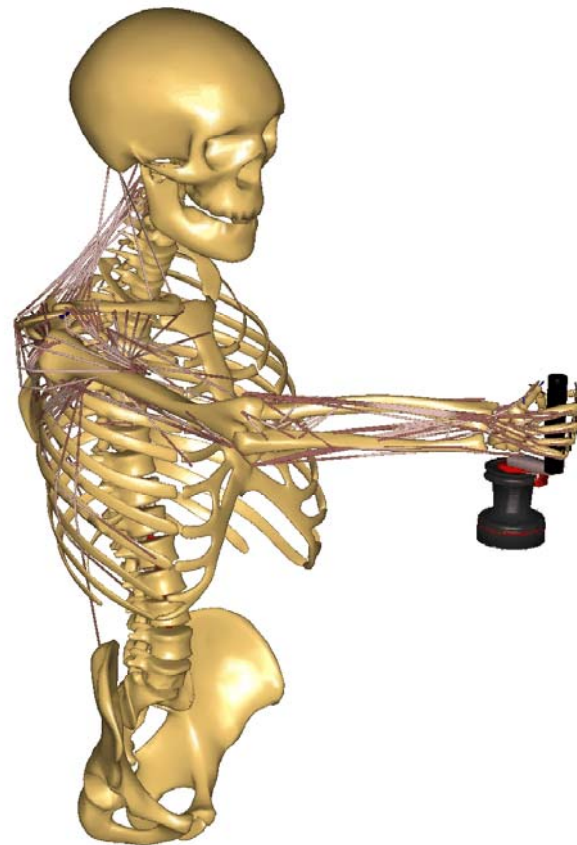
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Does a performance criterion defined based on muscle activity predict wide range of human movement?



Experimental setup of crank-rotation task  
[Ken Ohta et al., 2004]

$$I\ddot{\theta}_{\text{Crank}} + B\dot{\theta}_{\text{Crank}} = r e^T F$$

$$I = 0.02 \text{ Kg. m}^2$$

$$B = 0.37 \text{ Nms/rad}$$

$F$ : Hand contact force

- Four subjects
- Different starting points
- The angular velocity is zero at the beginning and ending of the task.
- 100 clockwise circular reaching movement at subjects' own pace.

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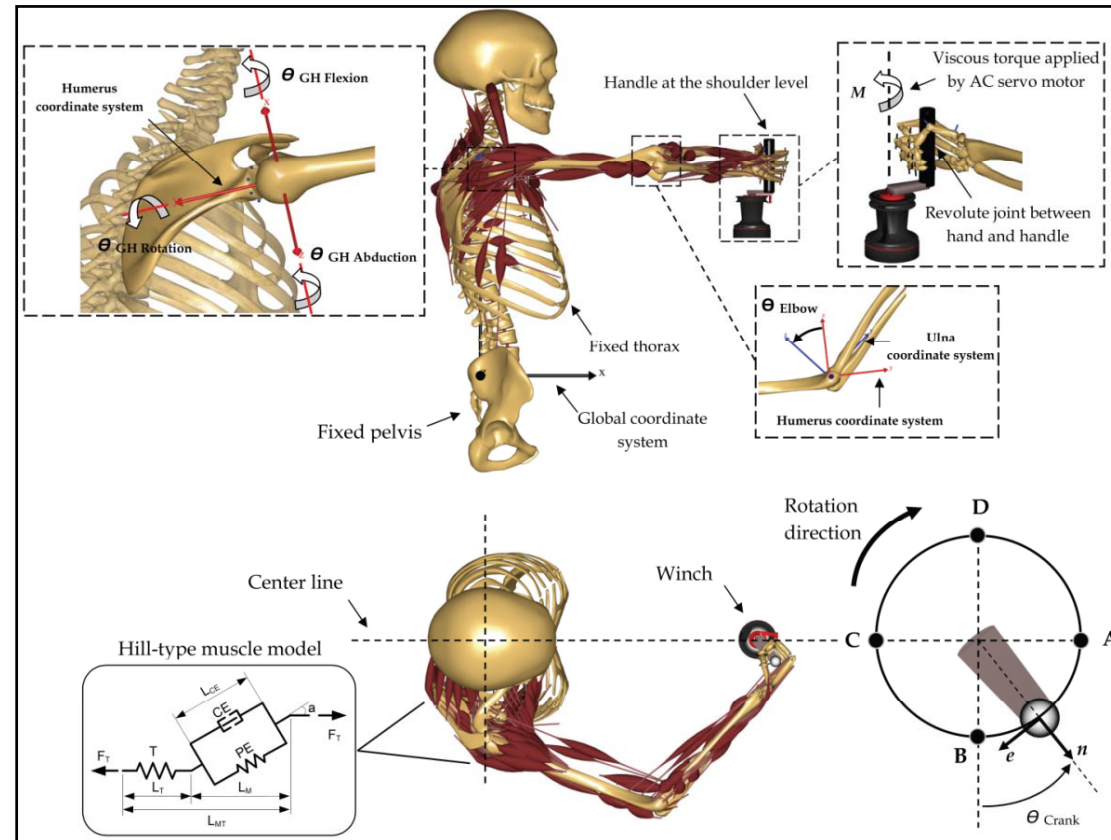
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□ Objective function:

$$F = \int_0^T \dot{E}_{Total}^M dt$$

$$\dot{E}^M = \frac{P_{mech}}{\mu}, \begin{cases} \mu = 0.25 & \text{for muscle shortening} \\ \mu = -1.2 & \text{for muscle lengthening} \end{cases}$$

□ Optimization:

Find:

$$q_i, \quad i \in \{1, \dots, n^{(C)}\}$$

To:

$$\text{minimize } \int_0^T \dot{E}_{Total}^M dt$$

S.t:

$$\begin{aligned} \theta_i^L &\leq \theta_i \leq \theta_i^U, & i &\in \{1, \dots, n^{(D)}\} \\ 0 &\leq f_i^{(M)} \leq N_i, & i &\in \{1, \dots, n^{(M)}\} \end{aligned}$$

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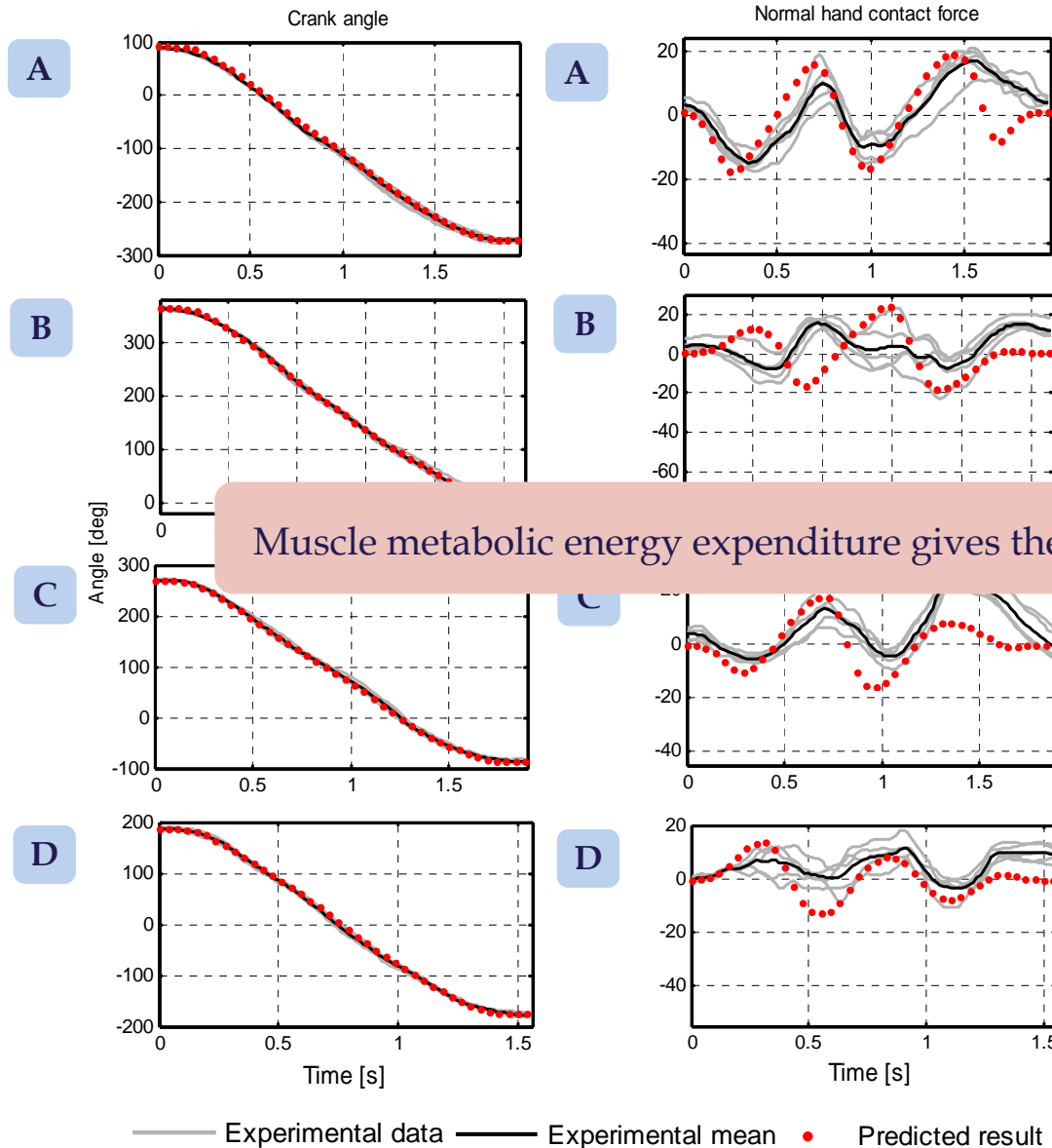
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	Crank angle	Normal hand contact force
Starting point A		
NRMSE	0.013	0.190
$r^2$	0.999	0.660
$M$	0.007	0.159
$P$	0.009	0.258
$C$	0.012	0.303
Starting point B		
NRMSE	0.007	0.522
$r^2$	0.999	0.005
$M$	0.006	0.404
$P$	0.003	0.503
$C$	0.003	0.645
Starting point C		
NRMSE	0.006	0.327
$r^2$	0.999	0.401
$M$	0.003	0.229
$P$	0.004	0.327
$C$	0.006	0.399
Starting point D		
NRMSE	0.009	0.466
$r^2$	0.999	0.443
$M$	0.002	0.072
$P$	0.008	0.358
$C$	0.009	0.365

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- Motivation
- Human models
- Simulation models
- State-of-the-art

## Posture/movement Prediction

- Parameterization
- Objective function
- Optimization
- Validation

## Results

- Example I
- Example II
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## Concluding remarks

## Future works

### Can we formulate the human movement prediction as an optimization problem?

The results of the jumping study indicated that human movement prediction can be treated as an optimization problem.

### What is the appropriate objective function for human movement prediction?

The results of the pedaling study indicated that for a movement under investigation a range of performance criteria should be evaluated in order to find an appropriate objective function.

### Does any single formulation predict a wide range of human posture/motion?

The results of the crank-rotation task indicated that an objective function defined appropriately based on muscle force/activity can predict natural human posture and movement.

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□ Defining a proper optimality criterion to solve the muscular load sharing problem remains a major challenge. One of the unanswered research questions is how the CNS chooses one of the possible muscle activation sets.

□ Although a performance criterion defined based upon the muscle activity seems to be a good choice, more investigation is needed to uncover how the CNS governs human posture and motions.

□ In order to investigate the capability of the inverse-inverse dynamics technique to predict more complicated movements, cases like normal and perturbed gait would be most relevant.