A new detailed lower extremity model



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This project was funded by the European Space Agency (ESA/ESTEC)

Presenters



Sebastian Dendorfer (Presenter)



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Outline

- Data for the new leg model
- Model details
- Leg validation
- Application:
 - Evaluation of tibia strains during walking in 1g and microgravity (study for the European Space Agency, ESA)



Aim



- Increase the level of detail in the lower extremity
- Template for more advanced joint kinematics (knee, ankle)



The Twente Lower Extremity Model

Comprehensive and consistent dataset from one donor (77 y, 1.74 m, 105 kg)

- Joint parameters
- Muscle parameters (optimum length, cross sectional area)
- Geometrical parameters (attachment sites, via-points)
- Inertia properties





¹Klein-Horsman, M. D. (2007), 'The Twente lower extremity model - consistent dynamic simulation of the human locomotor apparatus', PhD thesis, Universiteit Twente.

Data for the new leg

Most muscle and joint data is taken from the Twente study. Modified are:

- Joint axes and centers of ankle and subtalar joint
- Wrapping surface for Iliacus muscles adjusted to pelvis
- Muscle insertion points
 - Foot-muscles, insertion on the foot, via-points also on the shank
 - Gluteus Maximus Superior
 - Psoas
 - Iliopsoas muscles are taken from the old leg (connection to spine)





Muscles

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- 55 Muscles divided in 159 branches per leg
- 11 wrapping muscles (Gastrocnemius, Illiacus)

Muscles



New femur and tibia geometries were kindly supplied by P. Worsley, University of Southampton ANYBODY

Muscles – knee, ankle





Quadriceps Femoris (Vastus lat. (8), Vastus med. (10), Vastus int. (6), Rectus Femoris (2)) connected to the Patella



Validation

- Muscle moment arms
 - Derivative of the elongation of the muscle element with respect to the corresponding DOF (tendon excursion method)
- Maximal isometric joint moment
 - Ratio between applied moment at a certain DOF and the maximum muscle activity
- Gait analysis
 - Joint forces
 - Muscle activation patterns





Moment arms – subtalar joint

 Good correlation for most muscles with average literature values



Data reproduced from Klein et al., J Biomech, vol. 29, no. 1, pp. 21–30, Jan 1996.

Moment arms – ankle joint



Data reproduced from Klein et al., J Biomech, vol. 29, no. 1, pp. 21-30, Jan 1996.

Moment arms - knee joint



Data reproduced from Buford, W. L. et al. (1997), IEEE Trans Rehabil Eng 5(4), 367-379, red line: Anybody

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Moment arms – hip joint



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Moment arms – hip joint II





Validation – joint strength



500

400

300

200

100

-100

-200

→) moment (Nm)

the flexion (\leftarrow) / extension (-

Klein-Horsman, M. D. (2007), 'The Twente lower extremity model - consistent dynamic simulation of the human locomotor apparatus', PhD thesis, Universiteit Twente. red line: AnyBody

Normal walking

- Bodymodel includes new leg
- Hill-type 3 element muscle model
- Motion and force plate data given
- Load balanced by body forces and support for residuals



Normal walking





Normal walking





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Hip reaction forces – normal walking



Dataset: GaitUniMiami, Solver: MinMaxOOSolQP; e2 = 1000;

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Application: Analysis of tibia strains in normal walking and walking in microgravity

This project was funded by the European Space Agency (ESA)



Countermeasure exercise

- Tissue degeneration in space
- Treadmill walking
- Microgravity conditions
- Harness provides gravity replacement load (GRL)
- Questions:
 - Design
 - Level of GRL
 - Exercise
 - Efficiency of the exercise



http://www.spaceflight.esa.int/



Walking with harness – 0g

- Includes shoulder and waist harness¹
- Motion data given, ground reaction forces computed with simple contact
- Gravity replacement load:
 - 80% bodyweight
 - 100% bodyweight





¹ McCrory et al., Aviat Space Environ Med, vol. 73, no. 7, pp. 625–631, Jul 2002



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Results – harness walking

• Joint reaction forces and EMG patterns differ from normal walking





Results – harness walking

• GRF of normal walking and harness walking are similar in shape





Stress state in the tibia

- Point of evaluation: Preswing (stance phase)
 - High knee reaction forces
 - High muscle activity
- Including all forces and moments acting on the tibia (> 180)



Finite Element Model

- Linear, isotropic material model (E = 15000 MPa)
- Medullary canal is modelled, Epiphysis filled with cortical bone
- Rigid beams connecting muscle insertion points and tibia
- Ansys V11



Results - FEM

- Stresses are lower for both harness models
- Regions of highest stresses are similar

Lateral view



Results - FEM

Posterior view





Summary

- A very detailed leg model is proposed
- High level of detail in muscle definitions
- Validation results show a reasonable performance

Future:

- A more detailed validation for various applications
- A combined dataset for EMG and motion to analyze the activation patterns
- Advanced joint definitions in knee, ankle and foot



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We hope, that the model will be

- Downloaded
- Improved
- Validated for particular purposes
- Used for solving development and research questions



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